Wavelet-Based Preprocessing Methods for Mass Spectrometry Data

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Overview

- Background and Motivation
- Preprocessing Steps
 - Denoising using Wavelets
 - Baseline Correction/Normalization
 - Peak Detection/Quantification
 - Working with Average Spectrum
- Virtual Mass Spectrometer
- Simulation Study
- Conclusions

Statistical Issues for Mass Spectrometry Experiments

Experimental Design

 Blocking/RANDOMIZATION – reduce possibility of systematic bias polluting the data.

Preprocessing

- Remove systematic artifacts/noise from data
- Extract meaningful features (protein signal) : nxp matrix

Data Analysis/Discovery

- Analyze n x p matrix
 - Find which features are associated with exp. cond.
 - Build/validate classifier based on sets of features
 - Cluster samples/features
- Lots of existing methods available for this

$$Y_{i}(t_{j}) = B_{i}(t_{j}) + N_{i}S_{i}(t_{j}) + e_{ij}$$

Baseline Artifact
$$Y_i(t_j) = B_i(t_j) + N_i S_i(t_j) + e_{ij}$$

Baseline Protein Signal
$$Y_i(t_j) = B_i(t_j) + N_i S_i(t_j) + e_{ij}$$

$$Y_i(t_j) = \overbrace{B_i(t_j)}^{\text{Baseline}} + \underbrace{N_i}_{\text{Signal}} \underbrace{S_i(t_j)}_{\text{Signal}} + e_{ij}$$

$$\underbrace{Normal}_{\text{ization}}$$
Factor

$$Y_{i}(t_{j}) = \overbrace{B_{i}(t_{j})}^{\text{Baseline}} + \underbrace{N_{i}}_{\text{Signal}} \underbrace{S_{i}(t_{j})}_{\text{Signal}} + \underbrace{e_{ij}}_{\text{additive noise factor}}$$

$$e_{ij} \sim N\{0, \sigma^2(t_j)\}$$

Preprocessing

- Goal: Isolate protein signal $S_i(t_j)$
 - Filter out baseline and noise, normalize
 - Extract individual features from signal

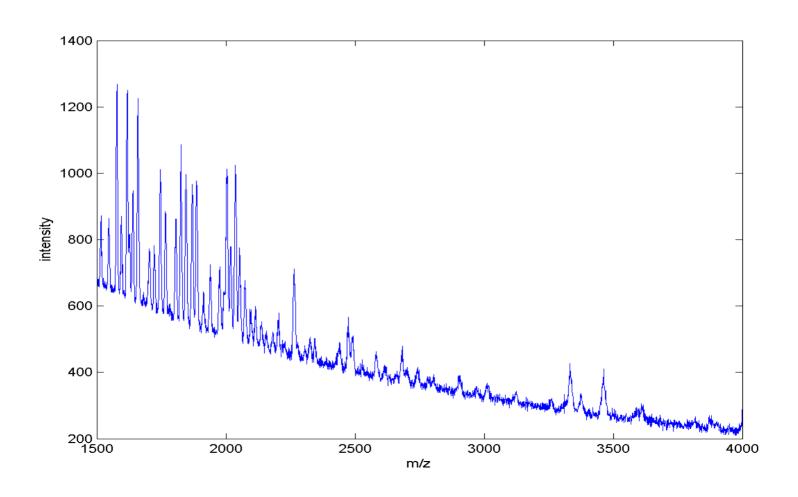
■ Problem:

- Baseline removal, denoising, normalization, and feature extraction are interrelated processes.
- Where do we start?

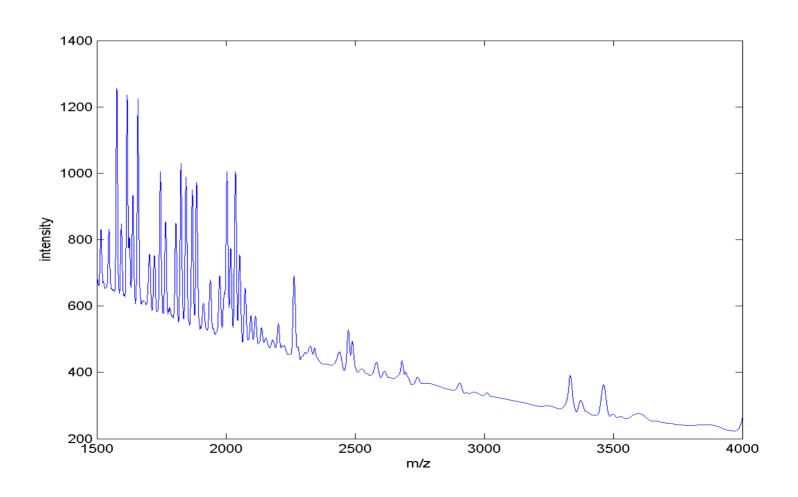
Denoising using Wavelets

- First step: Isolate noise using wavelets
 - Wavelets: basis functions that can parsimoniously represent spiky functions
 - Standard denoising tool in signal processing
- Idea: Transform from time to wavelet domain, threshold small coefficients, transform back.
 - Result: Denoised function and noise estimate
 - Why does it work? Signal concentrated on few wavelet coefficients, white noise equally distributed. Thresholding removes noise without affecting signal.
- Does *much* better than denoising tools based on kernels or splines, which tend to attenuate peaks in the signal when removing the noise.

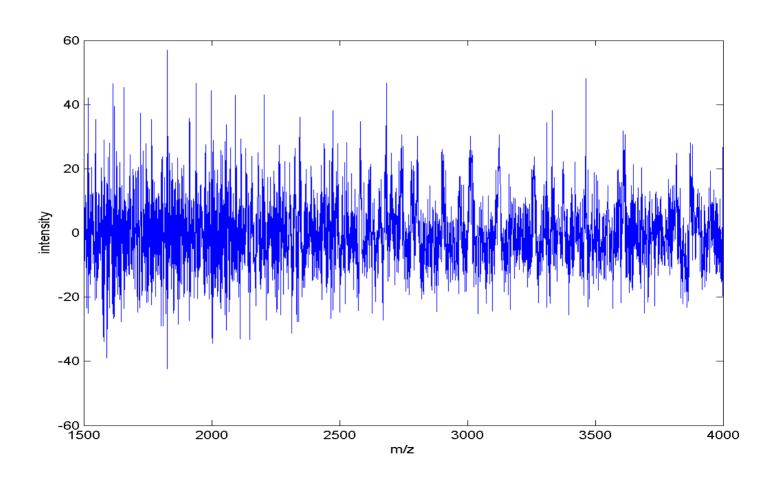
Raw Spectrum



Denoised Spectrum



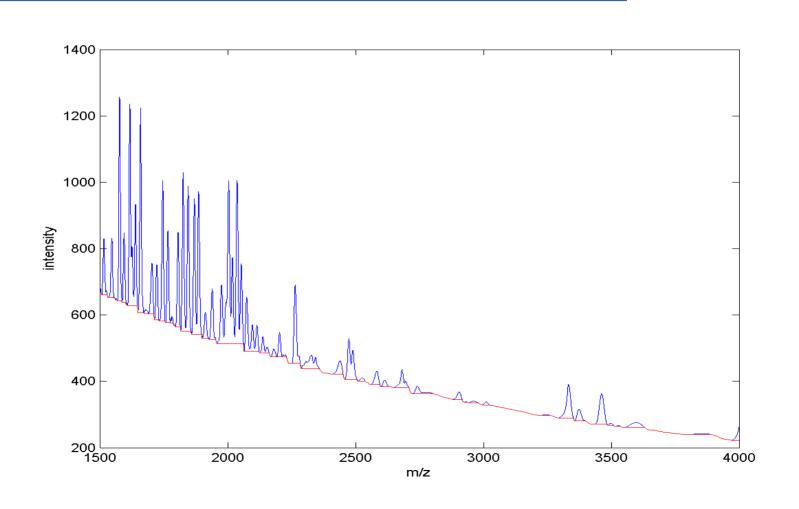
Noise



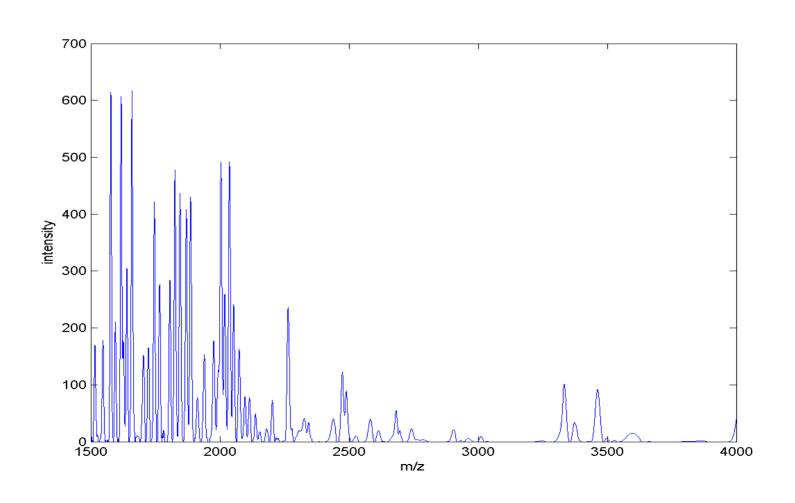
Baseline Correction & Normalization

- Baseline: smooth artifact, largely attributable to detector overload.
 - Estimated by monotone local minimum
 - More stably estimated after denoising
- Normalization: adjust for possibly different amounts of material desorbing from plates
 - Divide by total area under the denoised and baseline corrected spectrum.

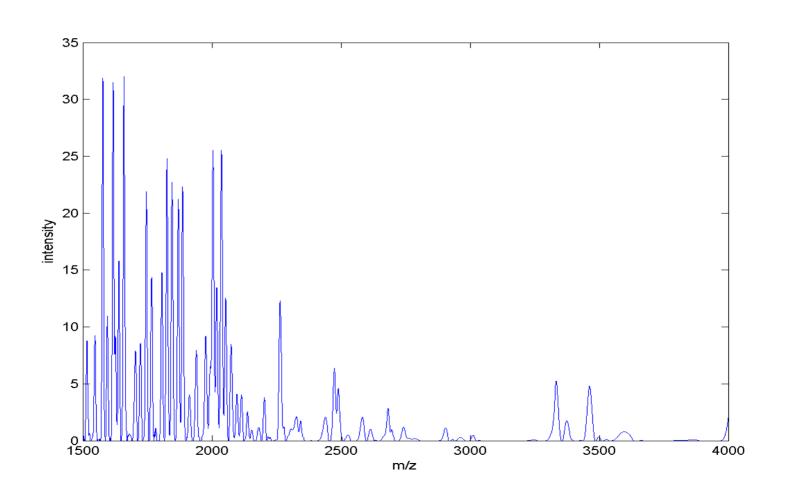
Baseline Estimate



Denoised, Baseline Corrected Spectrum



Denoised, Baseline Corrected, and Normalized Spectrum



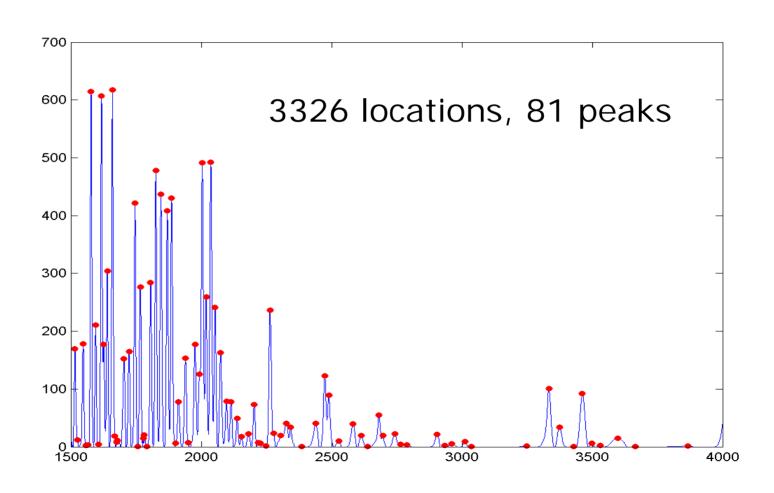
Protein Signal

- Ideal Form of Protein Signal: Convolution of peaks
 - Proteins, peptides, and their alterations
 - Alterations: isotopes; matrix/sodium adducts; neutral losses of water, ammonia, or carbon
- Limitations of instrument used means we may not be able to resolve all peaks.
- Advantages of peak detection:
 - Reduces multiplicity problem
 - Focuses on units that are theoretically the scientifically interesting features of the data.

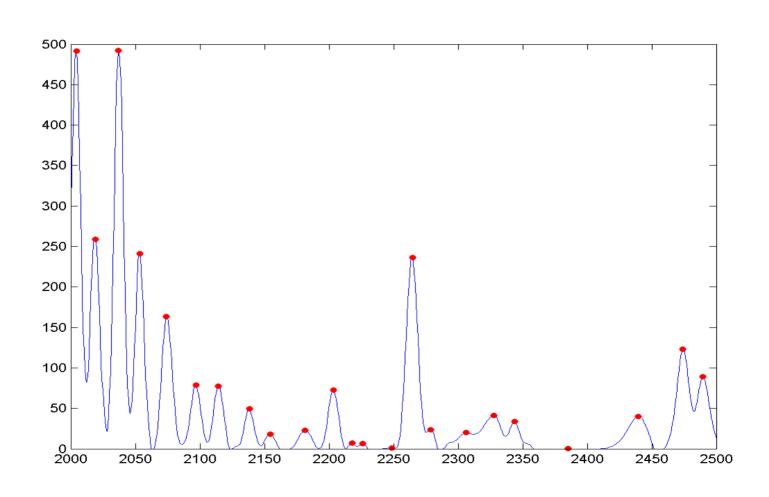
Peak Detection

- Easy to do after other preprocessing
- Any local maximum after denoising, baseline correction, and normalization is assumed to correspond to a "peak".
- May want to require $S/N>\delta$ to reduce number of spurious peaks.
 - We can estimate the noise process $\sigma(t)$ by applying a local median to the filtered noise from the wavelet transform.
 - Signal-to-noise estimate is ratio of preprocessed spectrum and noise.

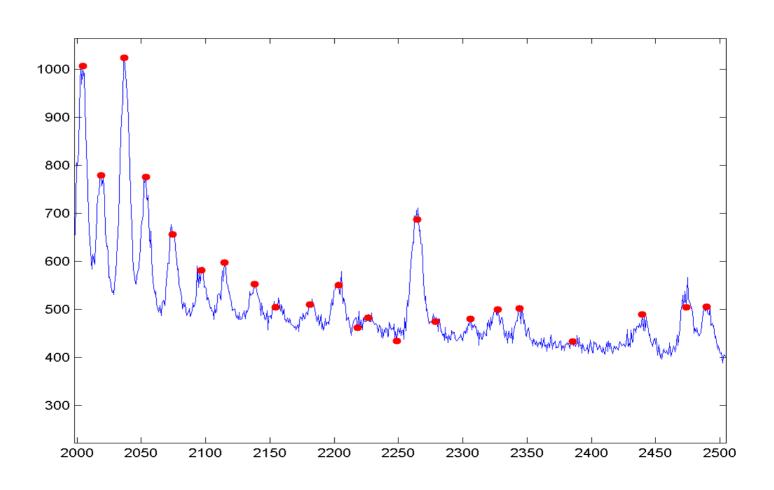
Peak Detection



Peak Detection (zoomed)



Raw Spectrum with peaks



Peak Quantification

- Two options:
 - Area under the peak: Find the left and right endpoints of the peak, compute the AUC in this interval.
 - Maximum intensity: Take intensity at the local maximum (may want to take log or cube root)
- Theoretically, AUP quantifies amount of given substance desorbed from the chip.
 - But it is very difficult to identify the endpoints of peaks

Peak Quantification

- The maximum intensity is a practical alternative
 - No need for endpoints, should be correlated with AUP
 - Physics of mass spectrometry shows that, for a given ion with m/z value x, there is a linear relationship between the number of ions of that type desorbed from plate and the expected maximum peak intensity at x.
- Problem with both methods: Overlapping peaks that are not deconvolvable
 - Local maximum at t contains weighted average of information from multiple ions whose corresponding peaks have mass at location t.
 - Major problem short of formal deconvolution, have not seen simple solution to this problem.

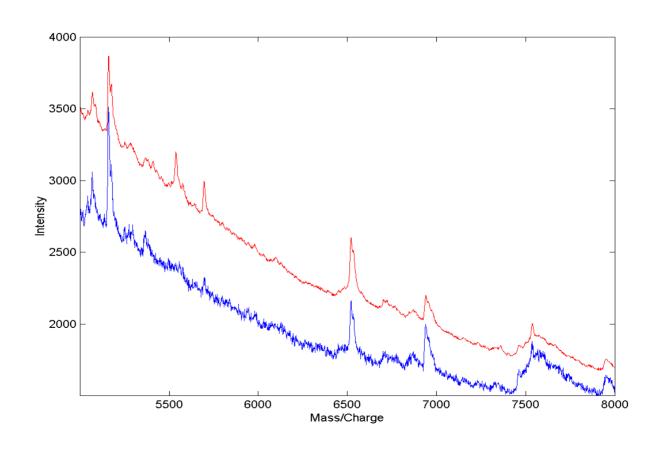
Peak Matching Problem

- If peak detection performed on individual spectra, peaks must be matched across samples to get n x p matrix.
 - Difficult and arbitrary process
 - What to do about "missing peaks?"
- **Our Solution:** Identify peaks on **mean spectrum** (at locations $x_1, ..., x_p$), then quantify peaks on individual spectra by intensities at these locations.

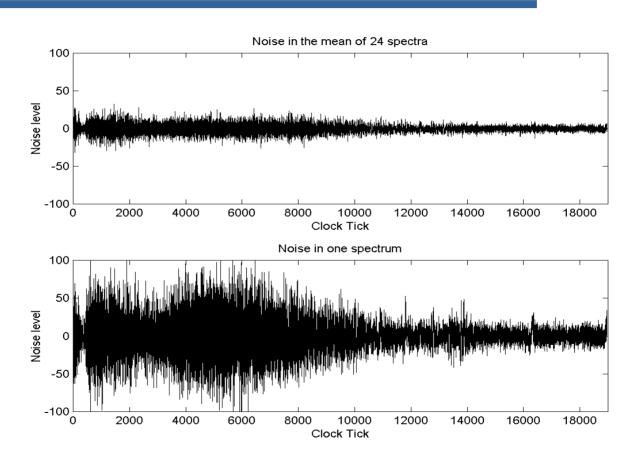
Advantages/Disadvantages

- Advantages
 - Avoids peak-matching problem
 - Generally more sensitive and specific
 - Noise level reduced by sqrt(n)
 - Borrows strength across spectra in determining whether there is a peak or not (signals reinforced over spectra)
 - Robust to minor calibration problems
- Disadvantage
 - Tends to be less sensitive when prevalence of peak < 1/sqrt(n).</p>

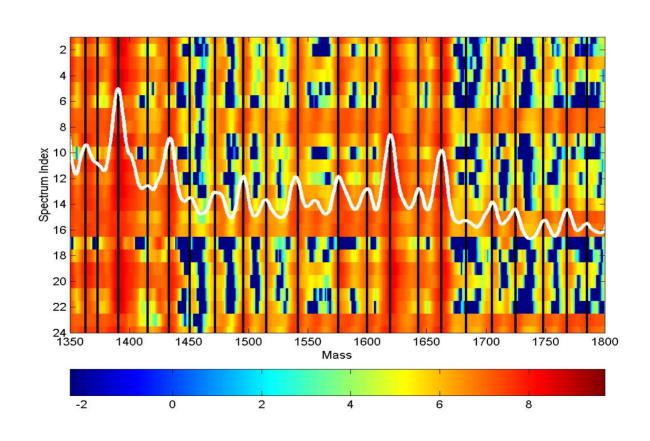
Noise reduced in mean spectrum



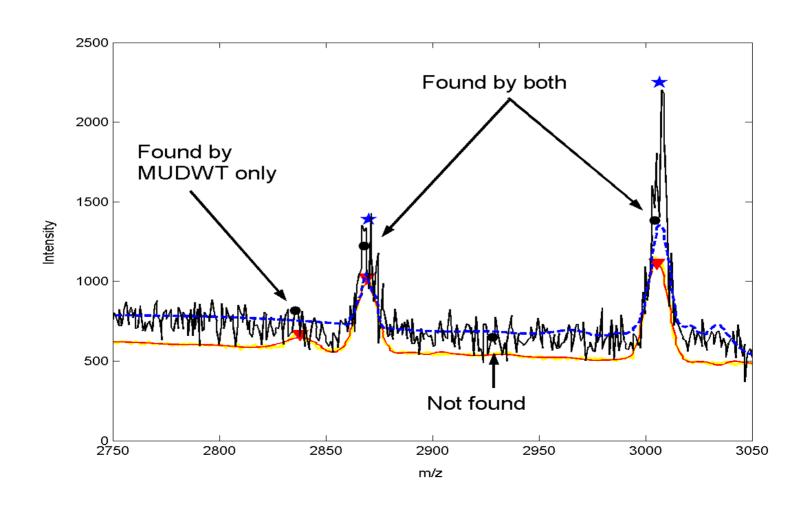
Noise reduced in mean spectrum



Peak detection with mean spectrum



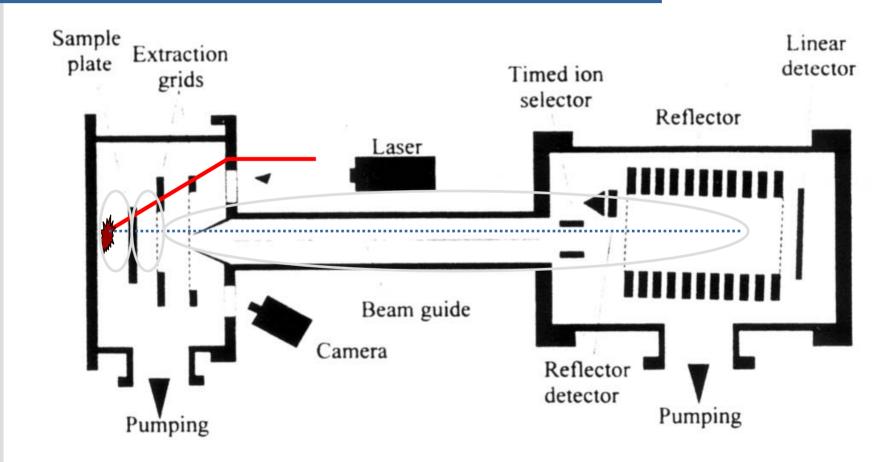
Sample Spectrum



Simulated spectra

- Difficult to evaluate processing methods on real data since we don't know "truth"
- Have developed a simulation engine to produce realistic spectra
 - Based on the physics of a linear MALDI-TOF with ion focus delay
 - Flexible incorporation of different noise models and different baseline models
 - Includes isotope distributions
 - Can include matrix adducts, other modifications

MALDI-TOF schematic



Vestal and Juhasz. J. Am. Soc. Mass Spectrom. 1998, 9, 892.

Modeling the physics of MALDI-TOF

Parameters

D₁ = distance from sample plate to first grid (8 mm)

 V_1 = voltage for focusing (2000 V)

 D_2 = distance between grids (17 mm)

V₂ = voltage for acceleration(20000 V)

L = length of tube (1 m)

 $v_0 = initial velocity ~ N(\mu, \sigma)$

v₁ = velocity after focusing

 δ = delay time

Equations

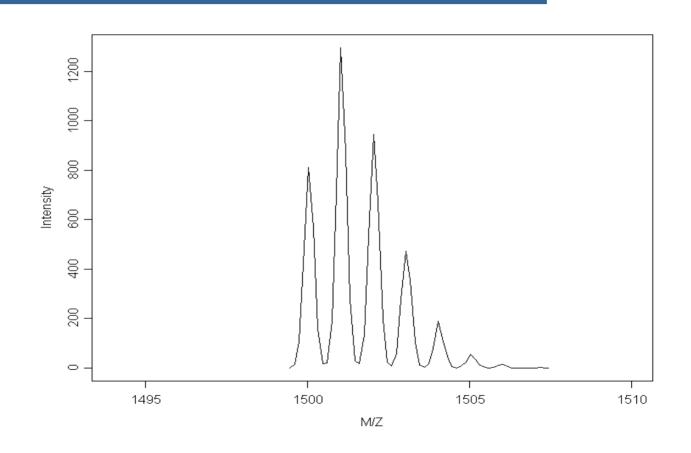
$$v_1^2 = v_0^2 + \frac{2qV_1}{mD_1}(D_1 - \delta v_0)$$

$$t_{DRIFT}^2 = L^2 / \left(\frac{2qV_2}{m} + v_1^2\right)$$

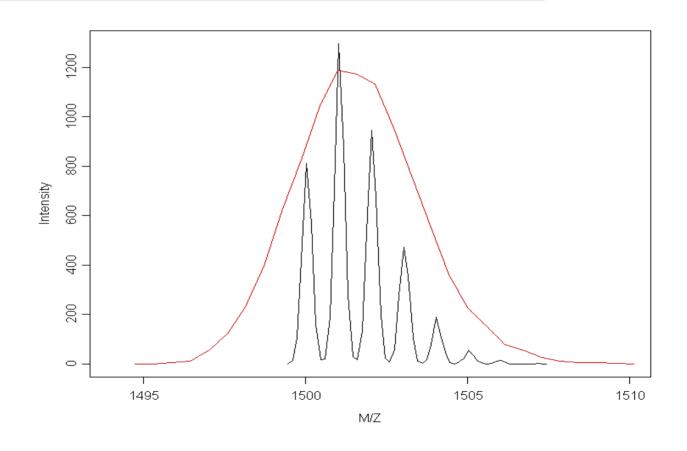
$$t_{ACCEL} = \frac{mD_2}{qV_2} \left(\frac{L}{t_{DRIFT}} - v_1 \right)$$

$$t_{FOCUS} = \frac{mD_1}{qV_1} (v_1 - v_0)$$

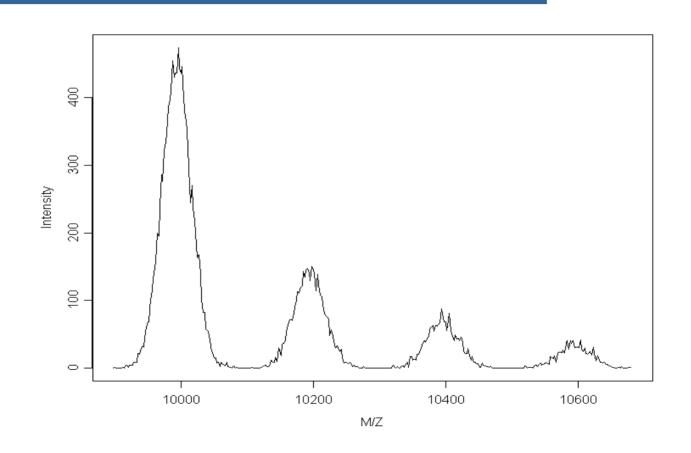
Simulation of one protein, with isotope distribution



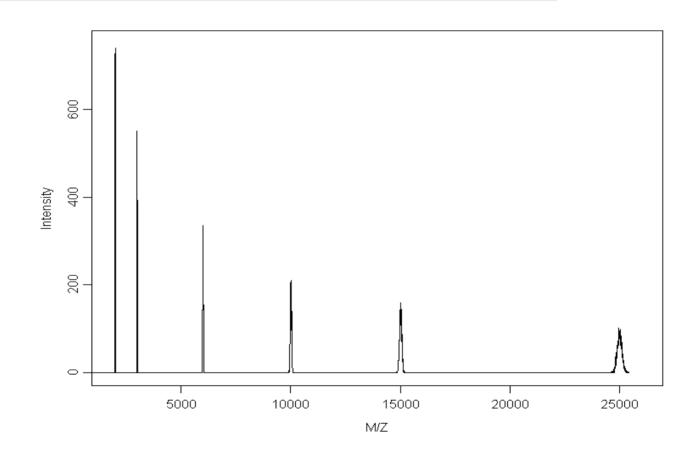
Same protein simulated on a low resolution instrument



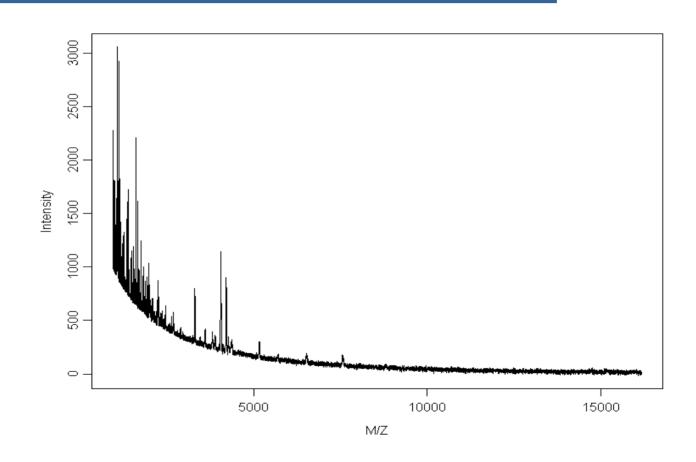
Simulation of one protein with matrix adducts



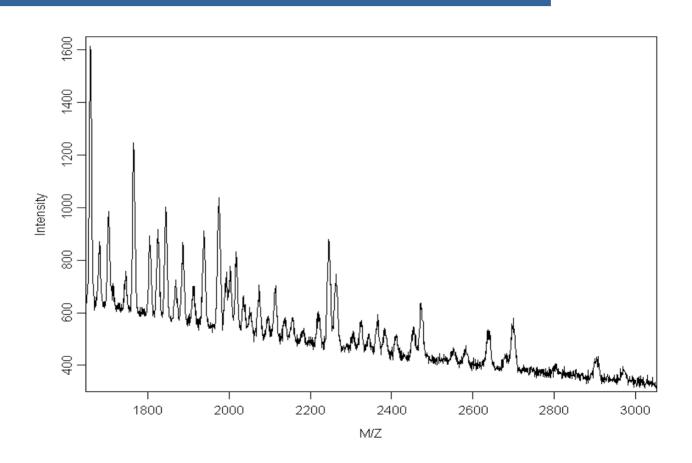
Simulated calibration spectrum with equal amounts of six proteins



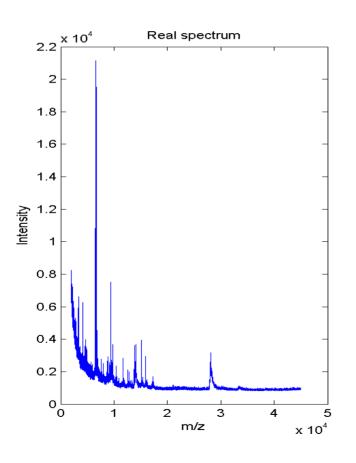
Simulated spectrum with a complex mixture of proteins

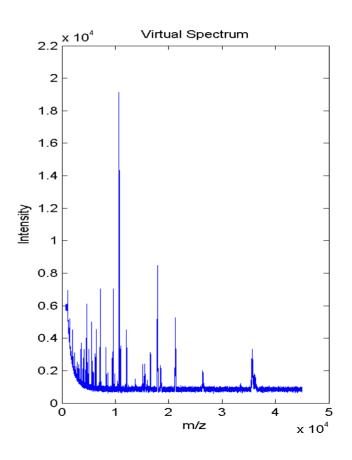


Closeup of simulated complex spectrum



Real and Virtual Spectra





Using Virtual Mass Spectrometer

- Input: virtual sample
 - proteins and peptides desorbed from sample
 - list of molecular masses w/ # of molecules
- Output: virtual spectrum
- Simulation Studies: virtual population
 - Defines distribution of proteins in proteome from which you are sampling
 - Assume p proteins; for each specify 4 quantities
 - major peak location (m/z of dominant ion)
 - prevalence (proportion of samples with protein)
 - abundance (mean # ions desorbed from samples w/ protein)
 - variance (var # of desorbed ions across samples w/ protein)

Simulation Study

- Generated 100 random virtual populations based on MDACC MALDI study on pancreatic cancer.
- For each virtual population, generated 100 virtual samples, obtained 100 virtual spectra.
- 3. Applied preprocessing and peak detection method based on individual and average spectra
- 4. Summarized performance based on sensitivity (proportion of proteins detected) and FDR (proportion of peaks corresponding to real proteins).
 - Tricky to do see paper for details.

Simulation Results Overall Results

	sensitivity	FDR	pv*
SUDWT	0.75	0.09	0.03
(indiv. spectra)			
MUDWT	0.83	0.06	0.97
(mean spectrum)			

^{*}pv=the proportion of simulations with higher sensitivity

Simulation Results By Prevalence

π:	<. 05 (14%)	. 0520 (16%)	. 2080 (40%)	>. 80 (30%)
sensitivity (SUDWT)	0.43	0.74	0.81	0.82
sensitivity (MUDWT)	0.38	0.74	0.93	0.97
pv (MUDWT)	0.25	0.49	1.00	1.00

Simulation Results By Abundance (mean log intensity)

log(μ):	< 9.0 (31%)	9.0-9.5 (27%)	9.5-10 (23%)	> 10 (19%)
sensitivity (SUDWT)	0.68	0.75	0.78	0.82
sensitivity (MUDWT)	0.78	0.84	0.85	0.88
pv (MUDWT)	0.97	0.89	0.84	0.78

Open problems: Preprocessing

- Better calibration?
 - Internal validation
- Better baseline correction?
- Alternative methods for normalization?
- Quality control/quality assurance?
- Best approach for quantification?

Open problems: Virtual Mass Spectrometry Instrument

- Include more alterations
 - Adducts and neutral molecule losses
 - Multiply-charged ions
- Develop more realistic model for baseline artifact
- Generalize to other instruments?

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